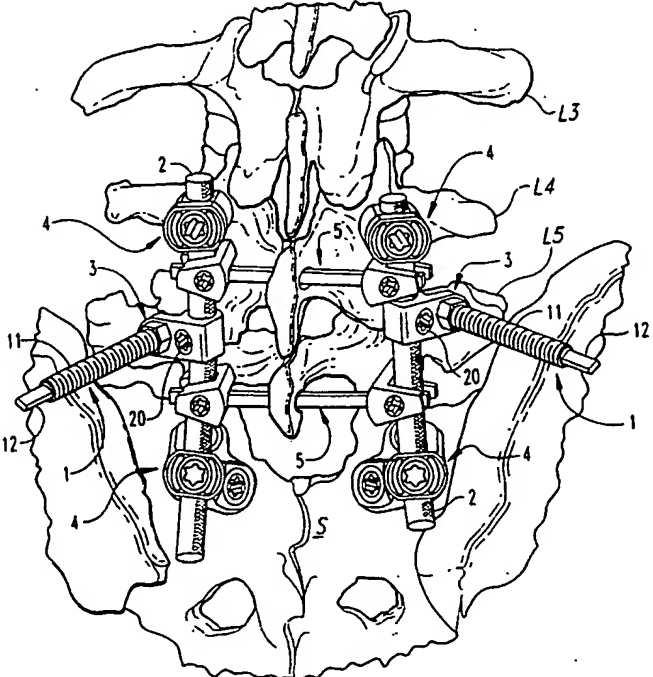


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<p>(21) International Application Number: PCT/US93/10966 (22) International Filing Date: 12 November 1993 (12.11.93) (30) Priority data: 92/13694 13 November 1992 (13.11.92) FR (71) Applicant (for all designated States except US): SOFAMOR DANEK GROUP, INC. [US/US]; 3092 Directors Row, Memphis, TN 38131 (US). (72) Inventor; and (75) Inventor/Applicant (for US only): HOPF, Christoph [DE/DE]; Draiserstrasse 155, D-6500 Mainz 1 (DE). (74) Agents: BECK, Michael, D. et al.; Woodward, Emhardt, Naughton, Moriarty &amp; McNett, Bank One Center/Tower, Suite 3700, 111 Monument Circle, Indianapolis, IN 46204 (US).</p>		<p>(81) Designated States: AU, BB, BG, BR, BY, CA, CZ, FI, HU, JP, KP, KR, KZ, LK, LV, MG, MN, MW, NO, NZ, PL, RO, RU, SD, SK, UA, US, UZ, VN, European patent (AT, BE, CH, DE, DK, ES, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE), OAPI patent (BF, BJ, CF, CG, CI, CM, GA, GN, ML, MR, NE, SN, TD, TG).  <b>Published</b> <i>With international search report.</i> <i>Before the expiration of the time limit for amending the claims and to be republished in the event of the receipt of amendments.</i></p>
<p>(54) Title: PEDICULAR SCREW AND POSTERIOR SPINAL INSTRUMENTATION</p> <p>(57) Abstract</p> <p>The instrumentation comprises for each lumbar vertebra (L5), two pedicular screws (1) having two screw threads (9, 11), one (9) of the screw threads corresponding to the region of penetration of the screw in the pedicle, two rods (2) having asperities respectively associated with a pedicular screw and secured to the latter by connection elements (3) provided with elements for clamping the rods. Each connection element (3) is in one piece and the screw thread (9) corresponding to the region of penetration of the screw in the pedicle terminates in an annular shoulder (16) against which the connection element bears which is separated by a smooth part (15) from the screw thread (11) outside the region of penetration in the pedicle. This instrumentation permits both returning the slipped vertebrae rearwardly and pivoting it in the desired direction of rotation, it being possible to carry out the derotation action slowly and by controlling the movement so that the surgeon achieves on the whole in the two movements an excellent precision in the repositioning of the vertebrae relative to the neighbouring vertebrae.</p> 		

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## PEDICULAR SCREW AND POSTERIOR SPINAL INSTRUMENTATION

The invention relates to lumbar osteosynthesis  
5 instrumentation for the correction of spondylolisthesis.

It is known that, substantially, spondylolisthesis is  
the forward displacement of a vertebra relative to its lower  
neighbour. In theory, any vertebra may be affected, but the  
fifth and the fourth lumbar vertebrae are the most commonly  
10 concerned.

Affecting more frequently women or young girls than men,  
spondylolisthesis is usually classified into five types:  
dysplastic, isthmian, traumatic, degenerative and  
pathological.

15 Its degree of seriousness is measured by the distance  
travelled through by the displaced vertebra with respect to  
its lower neighbour.

There are four stages:

The first stage is a displacement of a quarter of the  
20 antero-posterior diameter of the vertebral body.

The fourth stage corresponds to a complete displacement of  
the vertebral body.

The second and third stages are the intermediate stages.

Heretofore, although there are certain surgical  
25 techniques for the treatment of spondylolisthesis, either by  
the direct traction on the slipped vertebra, or by the  
screwing of the pedicles of this slipped vertebra, the

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reduction of the spondylolisthesis is not always satisfactory, above all in the cases of serious spondylolisthesis.

5 Surgery is indeed indicated for those who have a long past of lumbalgia or sciatica, in the case of evidence of a vertebral canal stenosis, a compression of the cauda equina or a subjacent motor lesion, or those whose spondylolisthesis rapidly evolves toward stage 3 or stage 4.

10 Generally, in surgery, an anterior or posterior vertebral fusion, laminectomy with decompression of the posterior structures and an excision of the hypertrophied mass of the fibrous tissue in the region of the lysis may be indicated.

15 In isthmian spondylolisthesis, the bilateral isthmian lyses are liable to be associated with a considerable pseudoarthrosis in relation with an emerging nerve root. The discal state in the region of the spondylolisthesis sometimes requires a radiculographic or discographic assessment. In vertebral canal stenoses, the decompression  
20 without fusion may be a surgical operation.

25 In actual fact, an effective orthopedic surgery consists in returning the vertebra not only onto the axis of the spine but also to a position which is as correct as possible relative to the neighbouring vertebrae. Over a period of time, or in the course of its displacement, this vertebra in fact might have been subjected to lateral thrusts which have caused it to pivot horizontally to a more or less large

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extent so that a correct repositioning of the vertebra of course implies its rearward return but also a derotation.

Attempts have already been made to correct spondylolisthesis, for example by means of devices consisting of two pedicular screws interconnected by a transverse plate which, by screwing a nut bearing against the plate, act solely by translation of the concerned vertebra for putting it into alignment with the neighbouring vertebrae.

Thus, the device disclosed in French patent 2 615 095 (87 06 864) employs two rods which are longitudinally fixed in the vertebral column with the aid of pedicular screws and each serve as support means for two screws having a double screw thread connected to the vertebra to be corrected.

These two double thread screws are transversely connected by a rigid plate constituting a bipedicular base. It is this transverse plate which permits acting on the vertebra to be corrected owing to the provision of a median opening for receiving traction forceps.

In fact, such a device does not permit acting in a sufficiently satisfactory manner, and experience has shown that a traction on the median part of the plate has for effect to rearwardly return the vertebra to be corrected too rapidly. Further, if this vertebra must be derotated, it has been found that the presence of the plate is liable to prevent the required derotation action owing to the fact that this induces at the same time a certain return of the

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vertebra.

Now, surgical experience has revealed that it is desirable to act slowly on the vertebra by acting on each one of the double thread screws independently, so that the surgeon can gradually adjust for each particular case his vertebra derotation and/or return action.

Moreover, such a device is relatively complex and costly owing to the number of its component parts which further increases the mounting difficulties encountered by the surgeon during the surgical operation. As concerns in particular the double thread screw, in addition to the fact that it is long and costly to produce, its implantation in the pedicles is not at all convenient.

Further, this double thread screw is subjected to extremely high shear stresses, mainly in the region of the junction with the instrumentation appliances or in the upper part of the screw thread.

An object of the invention is to provide a lumbar osteosynthesis instrumentation for the correction of spondylolisthesis, which permits both returning the vertebra to the rear and pivoting it in the desired direction of rotation. Another object of the invention is to provide a double thread pedicular screw so arranged as to overcome the aforementioned drawbacks while permitting mass production which is cheaper than in the case of screws known in the art which can only be produced on a small scale.

The osteosynthesis instrumentation according to the

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invention comprises, for each lumbar vertebra, two pedicular double thread screws, one thread of which corresponds to the region of penetration of the screw in the pedicle, two rods having surface asperities respectively associated with a pedicular screw and connected to the latter by connection elements provided with elements for clamping the rods.

According to the invention, each connection element is in one piece and the screw thread corresponding to the region of penetration of the screw in the pedicle terminates on an annular shoulder on which the connection element bears.

The derotation action exerted by means of this instrumentation has the advantage that it can be carried out slowly and with a certain amount of control over the movements, thereby affording on the whole in the two movements an excellent precision in the repositioning of the vertebra relative to its neighbouring vertebrae.

Further, the arrangement of a transverse shoulder into which tangentially fades the screw thread of the part of the screw serving to penetrate the pedicle, provides a reinforcement or strengthening resisting the shear stresses in this region. The continuous peripheral shoulder may also act as a support for an added part.

According to a particular feature of the invention, the end of the screw thread outside the part of the screw serving to penetrate the pedicle is extended by a screw threaded rod adapted to cooperate with an ancillary screwing

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device.

The instrumentation according to the invention comprises an ancillary device for screwing the pedicular double thread screw, this device bearing against the screw threaded  
5 extension of said screw. This ancillary device comprises a rod provided with an end grip and includes a tubular end part which is arranged to permit the insertion of the operating part of the double thread screw, has a conical free end part remote from the grip tapering toward the grip  
10 and is provided with at least one longitudinal slot. This ancillary device further comprises a tube freely slidable on the rod for the purpose of surrounding and gripping the conical end part of its tubular end part for the purpose of clamping it on the operating part of the pedicular screw.

15 With this ancillary device, the length of the operating screw thread is almost completely enclosed in the tubular end part and clamped owing to the action of the second tube when the latter surrounds the conical end part of the tubular end part. After having provided a prior bore in the  
20 pedicle, the surgeon can in this way easily screw the double thread screw in position.

Further features and advantages of the invention will be apparent from the following description with reference to the accompanying drawings which illustrate two embodiments  
25 of the invention by way of non-limitative examples.

In the drawings:

Fig. 1 is a perspective view from above of one



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embodiment of the lumbar osteosynthesis instrumentation according to the invention, mounted on the first lumbar vertebra and on the sacrum.

Fig. 2 is a partial perspective view of the instrumentation shown in Fig. 1.

Fig. 3 is an elevational view in the transverse direction, partly in section, of the instrumentation shown in Figs. 1 and 2.

Fig. 4 is an elevational view to a larger scale of a pedicular double thread screw which is part of the instrumentation shown in Figs. 1 to 3.

Fig. 5 is a perspective view of an embodiment of the ancillary device for mounting the pedicular screw shown in Fig. 4.

Fig. 6 is a perspective view to a larger scale of an alternative embodiment of the connection element between the osteosynthesis rod and the screw.

Fig. 7 is a sectional view taken on line 7-7 of Fig. 6.

The lumbar osteosynthesis instrumentation shown in Figs. 1 to 3 is adapted to correct spondylolisthesis by the posterior approach.

It comprises, for each lumbar vertebra to be corrected, for example the vertebra L5, two pedicular screws 1 having two screw threads, two cylindrical rods 2, preferably two rods of the so-called Cotrel type having surface asperities or knurling extending longitudinally along the concerned lumbar segment (vertebrae L5, L4 and sacrum S in the

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assembly shown in Fig. 1), connection elements 3 connecting each pedicular screw 1 to the adjacent rod 2, pedicular screws 4 for securing the rods 2 to the vertebra L4 and to the sacrum S, and devices 5 providing a transverse connection between the rods. All these elements except the pedicular screws 1 and the connection elements 3 are known per se and therefore need no special description.

Each connection element 3 has, when viewed in the transverse direction, a substantially L-shaped profile consisting of an enlarged base 3a in which is provided a through passage 10 receiving the rod 2 and having an axis X-X. This portion 3a has on one side a cylindrical surface and on the other side a planar surface and is extended by a thin portion 3b. The latter has two parallel planar surfaces and is provided with an opening 7 for the passage of the pedicular screw 1. The opening 7 consists of a cylindrical central part having an axis Z-Z extended on each side by two conical parts 7b, 7c opening onto the planar surfaces. The taper of these conical parts is such that it permits an inclination of the axis of the screw 11 relative to the axis Z-Z of about  $\pm 15^\circ$ , the angular limits of this axis corresponding to the axes Y-Y and Y'-Y' (Fig. 7). A tapped opening 6 transversely opens onto the bore or passage 10 and receives a screw 20 for radially clamping the rod 2. The surface 3c of the element 3 remote from the passage 10 is completely planar.

The element 3 constitutes the means for securing the rod

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2 and the means for screwing the screw 1. The distance between the axes of the screw 1 and rod 2 vary with the subject so that the surgeon can choose the most appropriate element 3.

5 Each screw 1 comprises from its point 8 a first screw threaded part 9 extending to the length of penetration of the screw 1 in the pedicular and a second screw threaded part 11 which is outside the region of penetration in the pedicle and is termed the "operating" part. On the side  
10 remote from the screw threaded part 9 the operating part 11 is extended by a profiled end portion 12, constituted for example by two flats 13 adapted to permit both the gripping of the double thread screw 1 and the screwing thereof by means of an ancillary device 14 (Fig. 5) which will be  
15 described hereinafter.

At the end remote from the profiled end portion 12, the screw threaded operating part 11 is extended by a short smooth region 15 terminating in a continuous peripheral shoulder 16 constituting the end of the screw threaded part  
20 9. This shoulder 16 bears against the planar surface of the element 3 which is the most remote from the screw threaded part 11, consequently the screw 1 cannot pass through the element 3.

The screw thread 18 of this screw threaded part is  
25 adjacent the shoulder 16 and the depth of the thread 21 close to the shoulder 16 gradually diminishes until it tangentially merges with or fades onto a cylindrical sector

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22 bordered by the shoulder 16 which thus forms a screw reinforcing region in this position. The shoulder 16 may act as a support for a device or an associated connection element 3.

5       The operating part 11 of the screw 1 is constituted by a metal screw thread of small pitch, for example between 0.5 and 2 mm and preferably between 0.8 and 1 mm, adapted to receive a nut 23 for clamping the connection element 3 against the shoulder 16.

10       This instrumentation has the following advantages:

      The fact that the connection element 3 is made in a single piece not only makes this element cheaper to manufacture but also simplifies the positioning of the element by the surgeon, and above all improves the strength  
15 of the connection between the rod 2 having asperities and the pedicular screw 1.

      As previously explained, the pedicular double thread screw 1 is subjected to high mechanical stresses of multiple origins; it must resist these various stresses for a  
20 relatively long period of time the duration of which depends on each patient. The screw 1 must therefore be as simple as possible to mount during the surgical operations, but must also have sufficient strength to withstand all the forces during and after the operation. Now, with the pedicular  
25 screws employed heretofore, it has been found that fractures generally occur in the region between the two screw threads. The invention remedies this situation by terminating the

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screw thread 18 for anchoring in the pedicle in the substantially tangential region 22. Consequently, the screw thread 18 does not "open out" onto the shoulder 16 for supporting the connection element 3 and consequently ensures  
5 that this shoulder 16 has a peripheral continuity and a sufficient supporting thickness. This supporting thickness thus affords the maximum mechanical resistance to the forces transmitted to the connection element 3 and therefore exerted by the latter.

10 Another advantage afforded by this arrangement of the anchoring screw thread 18 resides in the fact that, when it is desired to effect a bicortical anchorage by reaching the opposite cortical part of the vertebra and with the screw thread length corresponding to the length of the passage  
15 through the vertebra, the surgeon is informed of the desired final position of the screw thread. The stoppage of the latter in its upper part indeed constitutes a warning in that the surgeon must suddenly exert a higher torque. He must therefore stop his screwing effort.

20 Owing to the provision of the profiled end portion 12, the engagement of the pedicular screw 1 by the ancillary device 14 no longer occurs in the central region of the screw, as described in said patent 2 615 095, but at the free end of the screw. This end region may be in the form  
25 of two flats 13 provided on a smooth, or optionally screw threaded, end part to permit the ancillary device 14 to act on the screw.

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This ancillary device comprises a rod 24 provided with a tubular end part 25 and, at its opposite end, a manual grip 26. The tubular part 25 is so dimensioned as to permit the insertion therein of the operating part 11 of the screw 1, and the ancillary device 14 is completed by a tube or sleeve 27 coaxial with the rod 24 and slidably mounted on the latter so as to be capable of surrounding the tubular part 25 at the end of its travel.

The tubular part 25 is provided with longitudinal slots 28 starting at its free end, for example three slots as illustrated, extending along a part of the length of the region 25. The free end portion 29 of the latter is conical and tapers in the direction toward the grip 26. Beyond the slots 28, at a certain distance from the latter, there is provided a hollow profile matching the profiled end portion 12 of the screw, for example, as shown in Fig. 5, two flats 31 whose longitudinal surfaces are parallel. The two flats 31 are adapted to receive corresponding flats 13 of the screw 1 and thus lock the latter against rotation after the insertion of the operating part 11 in the tubular part 25. In the direction toward the conical end part 29, the flats 31 are extended by longitudinal recesses 32 for receiving the operating part 11 of the screw 1. Lastly, in order to permit a visual checking of the position of the profiled end portion 12 on the flats 31, the tubular part 25 is provided with a transverse opening 33 in the region of the flats.

When the operating part 11 is inserted in the tubular

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part 25 with its end portion 12 locked against rotation between the flats 31, the surgeon slides the tube 27 along the tubular part 25 until the conical end portion 29 is made to grip round the operating part 11, the tapered portion 29 thus constituting a holding chuck for the screw 1. The two flats constitute additional means for preventing a reverse rotation of the pedicular screw 1 in the ancillary device 14. The ancillary device 14 also serves to screw the nut 23 clamping the screw 1 in the connection element 3. It is provided in its end 29 with a corresponding recess for engaging this nut 23.

The instrumentation just described is used in the following manner.

Before placing in position the support rods 2, which are for example the known Cotrel rods (Registered Trademark), the surgeon suitably anchors with his ancillary device 14 the double thread screws 1 in each of the pedicles of the vertebra L5 to correct. Then he secures the support rods 2 to the neighbouring vertebrae, or, as in the embodiment shown in Fig. 1, to the sacrum S and vertebra L4. Then he firmly fixes the connection elements 3 to the rods 2 by means of a radial clamping screw 20 (Fig. 1).

At this stage, the two transverse connection rods 5 are not yet installed. In order to correct the vertebra L5, i.e. to return it rearwardly (spondylolisthesis) and/or derotate it, the surgeon acts on the nuts 23 clamping the connection elements 3 by means of an ancillary device and

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preferably two ancillary devices, each being disposed on one of the nuts 23 of the two screws 1. He is now free to act, as desired, more on the screwing of one of the nuts 23 than on the screwing of the other, depending on the movement he wishes to impart to the vertebra L5, as he is free to act in an identical manner on the two nuts 23.

Each time the surgeon acts on one of the nuts 23, he exerts by the bearing of the screw thread-nut system on the connection element 3 firmly connected to the support rod 2, a traction on the vertebra L5 in a direction toward the connection element 3. When he acts on a single one of the nuts 23, he also produces a slight rotation of the vertebra L5 about itself. When he acts equally on both nuts 23, he produces a rearward return of the vertebra L5.

In all cases, the fine pitch of the screw thread 11 supporting the correction nut 23 permits acting very progressively on the vertebra. When the vertebra is finally in the position required by the surgeon, the latter severs the double thread screw 1 above the nut 23. The severing of the rod deforms the screw thread 11 and this subsequently prevents the unscrewing of the nut 23.

It is only at this moment that the transverse rods 5 interconnecting the rods 2 can be mounted, thereby achieving a rectangulation of the whole final instrumentation.

The instrumentation according to the invention is easier to place in position by the surgeon than that disclosed in said French patent 2 615 095, cheaper as concerns the



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fabrication of the screw, and more reliable in use; it no longer requires a transverse handling plate in the region of the connection elements 3. The screwing of the pedicular screws 1 by their profiled end portions 12 rather than by their central regions as in the aforementioned prior instrumentation, is also more convenient for the surgeon.

It must be understood that the scope of the invention is not intended to be limited to the described embodiments and various modifications may be made. For example, it is obvious that the end portion 12 may have any suitable profile other than that described, the same being true of the corresponding two flats 31 of the ancillary device 14.

Likewise, in the alternative embodiment shown in Fig. 6, the connection element 3 may be constructed to have, as viewed in the transverse direction, a substantially L-shaped profile and be disposed in such manner that its planar surface 3c (in contact with the nut 23 in Fig. 3) is inverted, by turning the element round, so as to be closer to the adjacent vertebra.

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WHAT IS CLAIMED IS:

1. Lumbar osteosynthesis instrumentation for the correction of spondylolisthesis by a posterior approach, comprising in combination for each lumbar vertebra, two pedicular screws each having a first screw thread and a second screw thread, said first screw thread corresponding to a region of penetration of said pedicular screw in the pedicle of the vertebra, two cylindrical rods each associated with a respective pedicular screw, connection elements each interconnecting each rod and the associated pedicular screw, an annular bearing shoulder for the connection element interposed between said first and second screw threads on each pedicular screw, clamping elements each associated with a respective connecting element for clamping the respective rod, said first screw thread of each pedicular screw terminating on said shoulder and said shoulder being separated by a smooth part from said second screw thread outside said region of penetration of said first screw thread in said pedicle.

2. Instrumentation according to claim 1, wherein each connection element has a substantially L-shaped profile and a planar surface and is disposed, when the instrumentation is placed in position, in such manner that said planar surface is placed as close as possible to the adjacent vertebra.

3. Instrumentation according to claim 1, wherein each connection element has a substantially L-shaped profile and

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a planar surface and is disposed, when the instrumentation is placed in position, in such manner that said planar surface is spaced away from the adjacent vertebra.

4. Instrumentation according to claim 1, wherein each connection element has two opposed planar surfaces and is provided with an opening for receiving the respective pedicular screw, said opening having a cylindrical central part extended at both ends by conical parts each opening out onto a respective one of said planar surfaces of said connection element.

5. Instrumentation according to claim 1, comprising a profiled end portion at an end of said second screw thread remote from said shoulder of each pedicular screw for cooperation with an ancillary screwing device.

6. Instrumentation according to claim 1, wherein each second screw thread has a pitch of substantially 0.5 to 2 mm.

7. Instrumentation according to claim 1, wherein each second screw thread has a pitch of 0.8 to 1 mm

8. Instrumentation according to claim 5 in combination with an ancillary device for screwing each pedicular screw by a part thereof, termed operating part, outside said region of penetration of said pedicular screw in said pedicle, said ancillary device comprising a rod provided with an end grip and a tubular end part which is arranged to permit the insertion therein of said operating part of the respective pedicular screw, has a conical free end portion

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remote from said grip and tapering in a direction toward said grip, and defines at least one longitudinal slot, and a tube freely slidably mounted on said rod of said device so as to be capable of surrounding and gripping said conical  
5 free end portion of said tubular end part for causing it to grip said operating part of said pedicular screw.

9. Instrumentation according to claim 5 in combination with an ancillary device for screwing each pedicular screw by a part thereof, termed operating part, outside said  
10 region of penetration of said pedicular screw in said pedicle, said ancillary device comprising a rod provided with an end grip and a tubular end part which is arranged to permit the insertion therein of said operating part of the respective pedicular screw, has a conical free end portion  
15 remote from said grip and tapering in a direction toward said grip, and defines at least one longitudinal slot, and a tube freely slidably mounted on said rod of said device so as to be capable of surrounding and gripping said conical free end portion of said tubular end part for gripping and  
20 tightening a nut.

10. Instrumentation according to claim 9, wherein said ancillary device comprises, in said tubular end part and beyond said conical free end portion, a hollow profile matching said profiled end portion of said pedicular screw  
25 so as to prevent rotation of said pedicular screw relative to said tubular end part.

11. Instrumentation according to claim 10, wherein said

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hollow profile defines two flats having parallel surfaces and said profiled end portion of said pedicular screw defines two flats having parallel surfaces cooperative with said two flats of said hollow profile.

5        12. Instrumentation according to claim 10, wherein said hollow profile is extended in a direction toward said conical free end portion by longitudinal recesses for receiving said second screw thread of said pedicular screw.

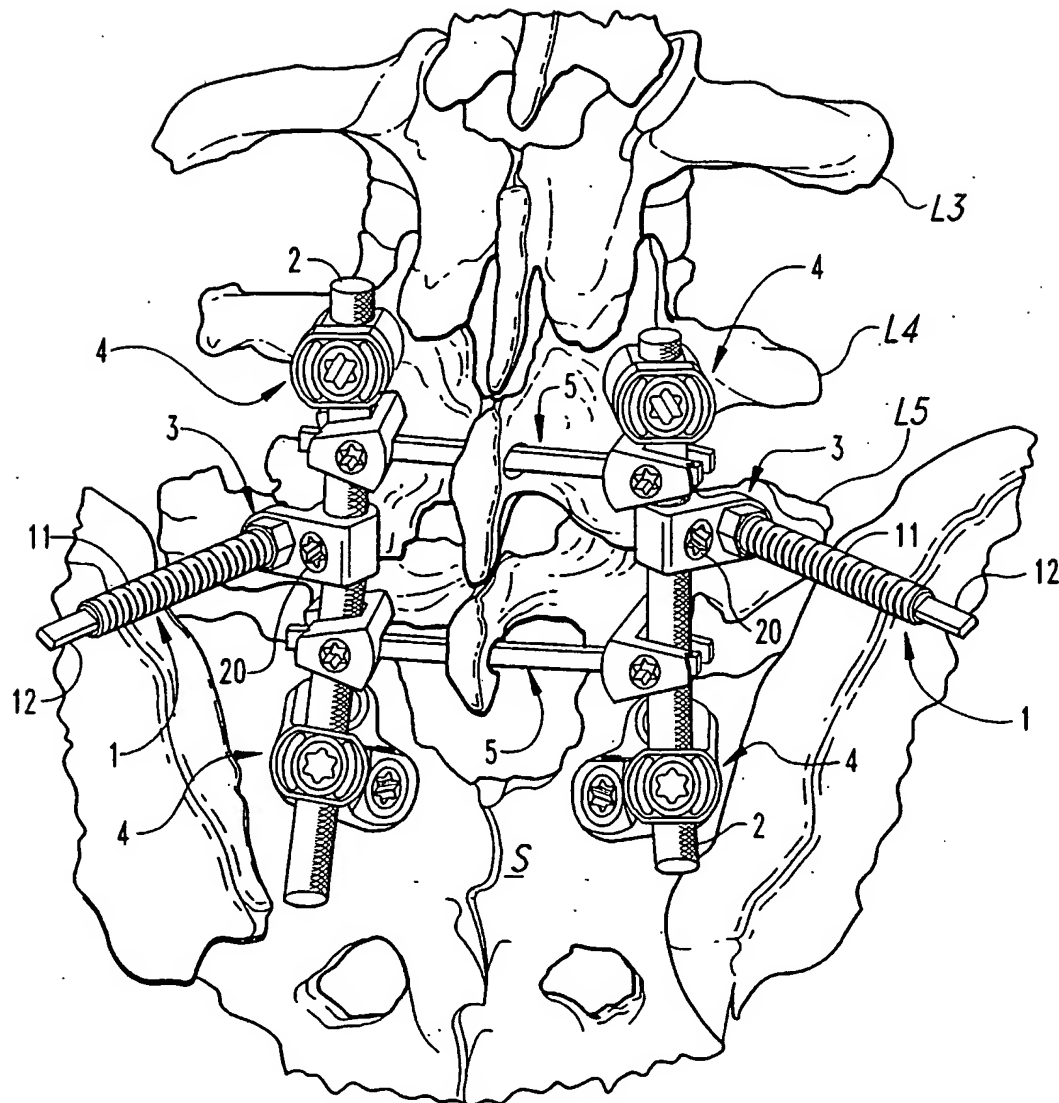
10        13. Instrumentation according to claim 10, comprising a transverse opening in said tubular end part in the region of said hollow profile for a visual checking of the engagement of said pedicular screw with said hollow profile for preventing relative rotation.

15        14. Pedicular screw for use in an osteosynthesis instrumentation, said pedicular screw comprising a first screw thread and a second screw thread and a transverse shoulder interposed between said two screw threads for supporting a connection element forming part of said instrumentation, said first screw thread being for screwing  
20        into the pedicle of a vertebra and having an end thread helix which fades tangentially on a cylindrical sector of said transverse shoulder.

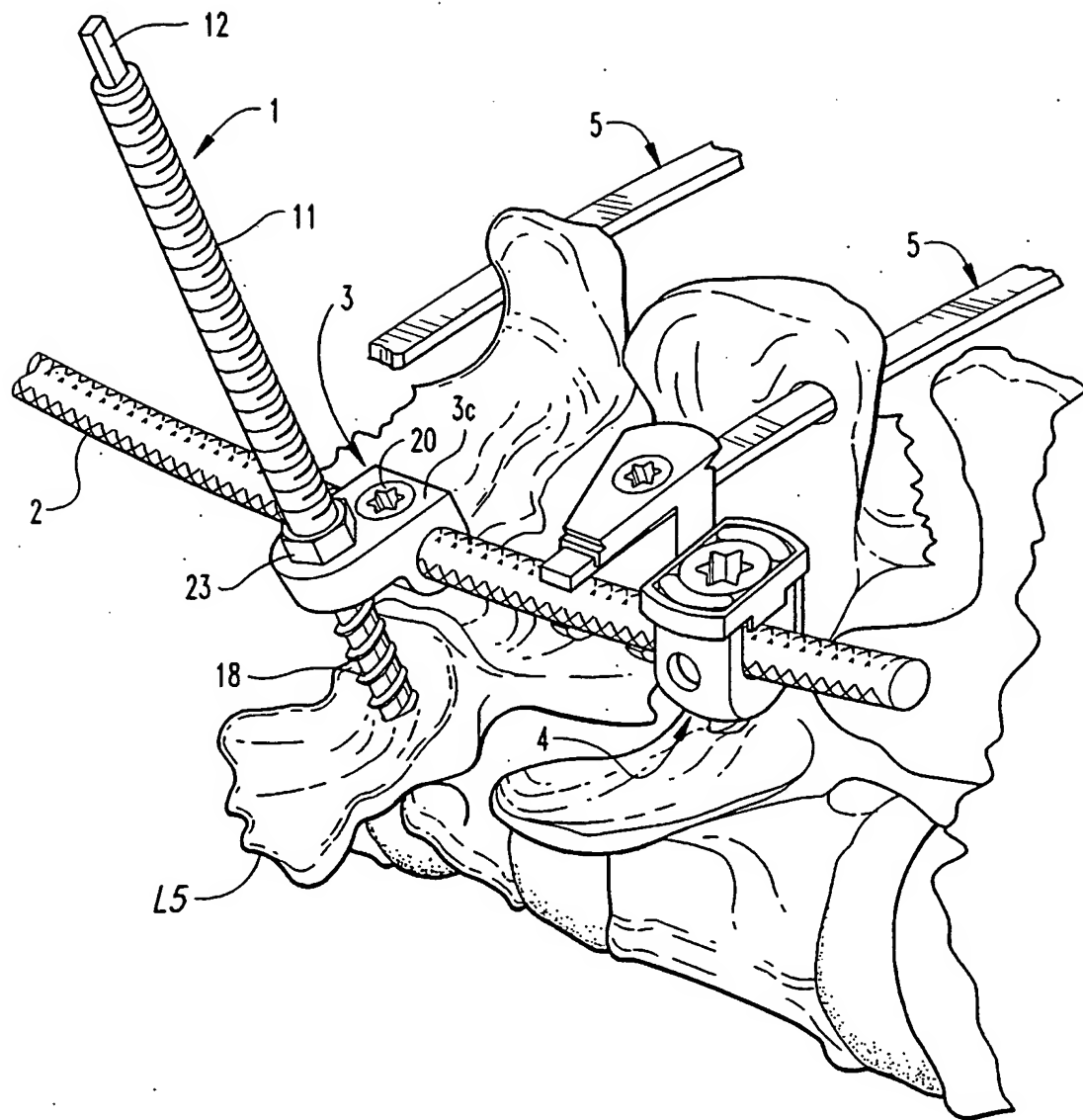
25        15. Ancillary device intended for an osteosynthesis instrumentation for screwing a pedicular screw which forms part of said instrumentation and comprises a first screw for screwing into the pedicle of a vertebra and a second screw constituting an operating part, said ancillary device

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comprising a rod which has a tubular end part and terminates  
in an end grip, said tubular end part being so dimensioned  
as to permit the insertion therein of said operating part of  
said pedicular screw, said tubular end part having a conical  
5 free end portion remote from said grip which tapers in a  
direction toward said grip, and at least one longitudinal  
slot, said ancillary device further comprising a tube freely  
slidably mounted on said rod of said ancillary device for  
the purpose of surrounding and gripping said conical end  
10 portion of said tubular end part and causing it to grip said  
operating part of said pedicular screw.

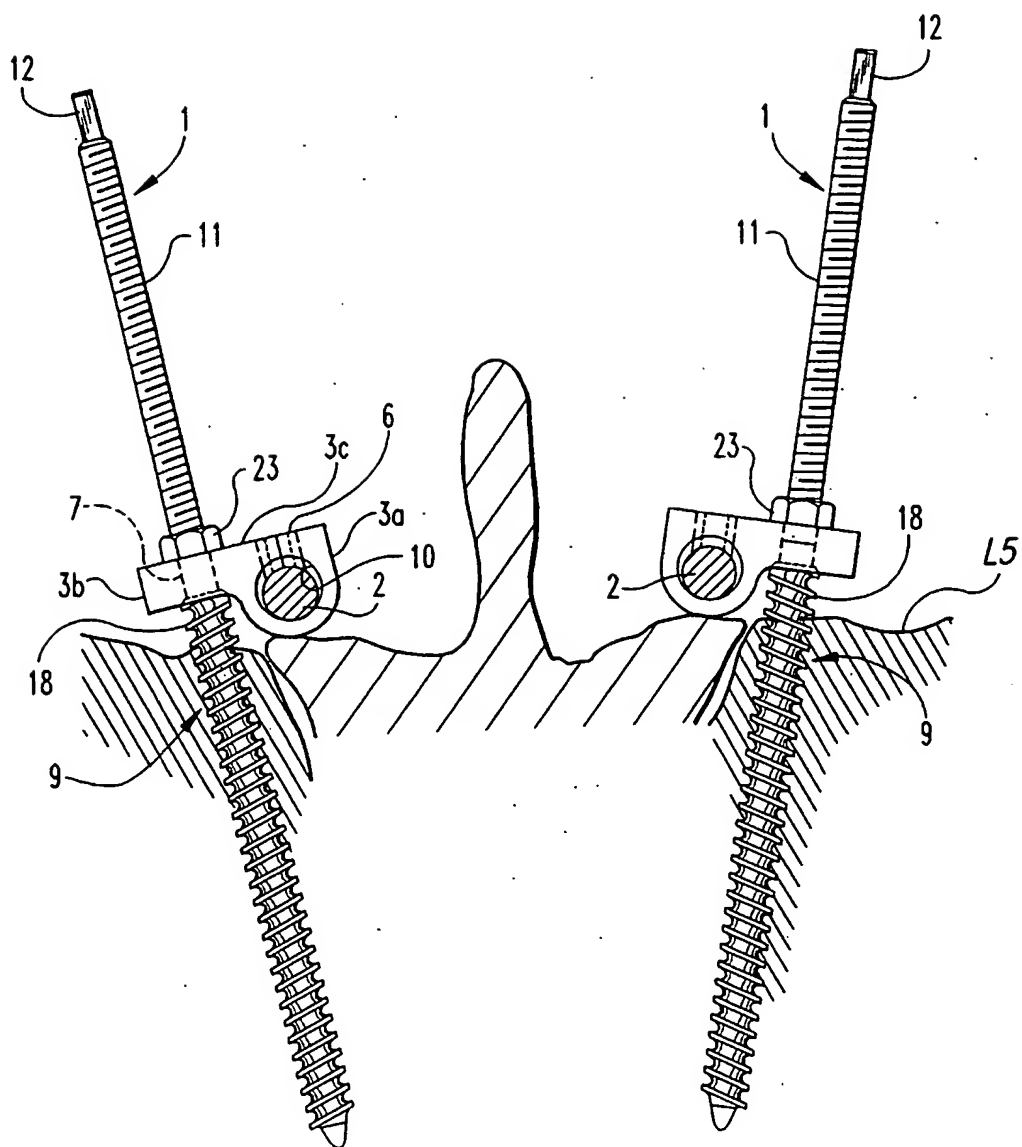
**Fig. 1**

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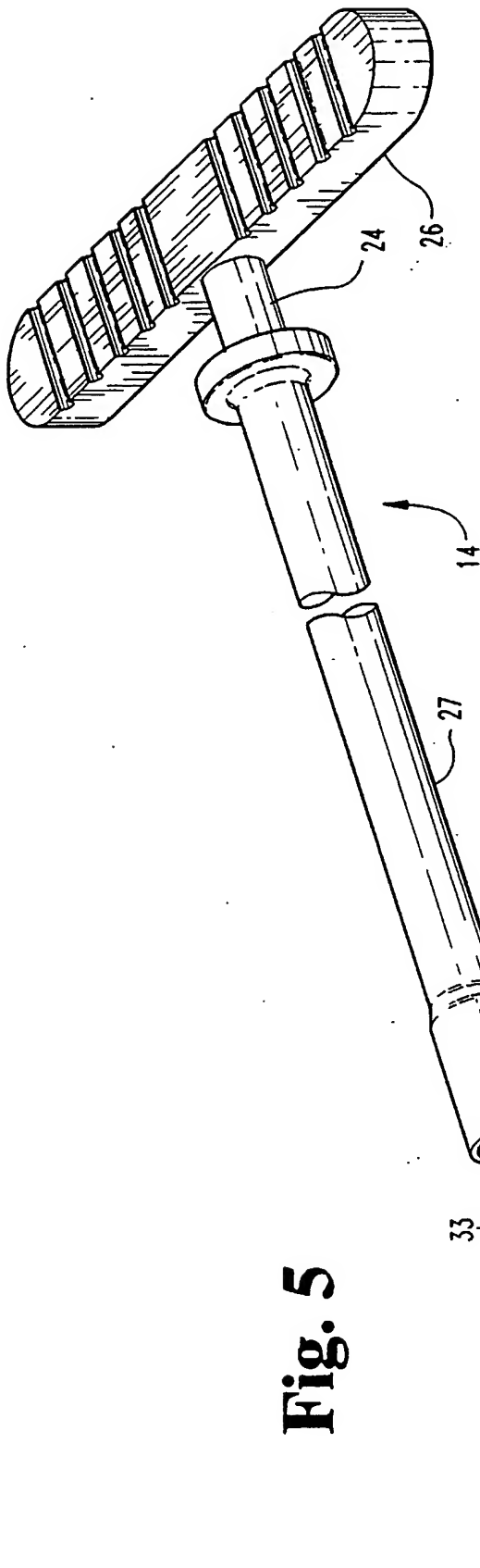


**Fig. 2**



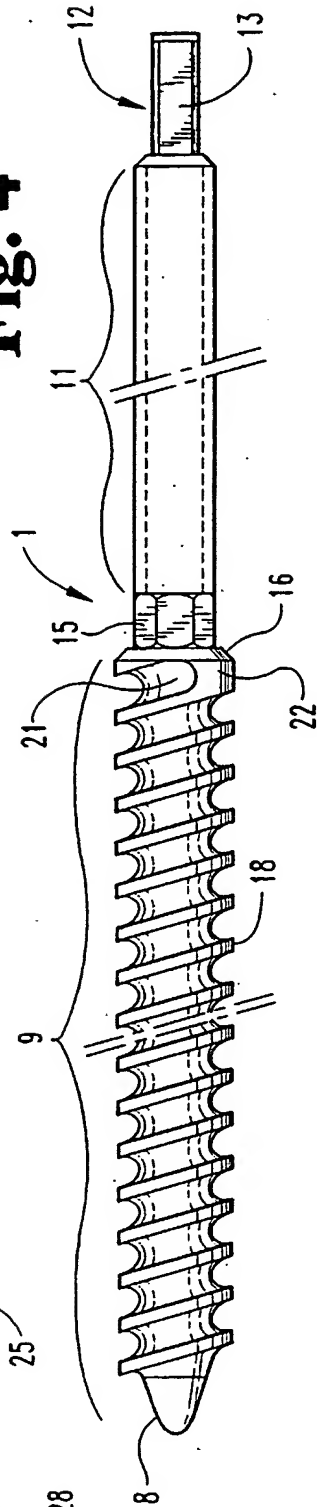
**Fig. 3**

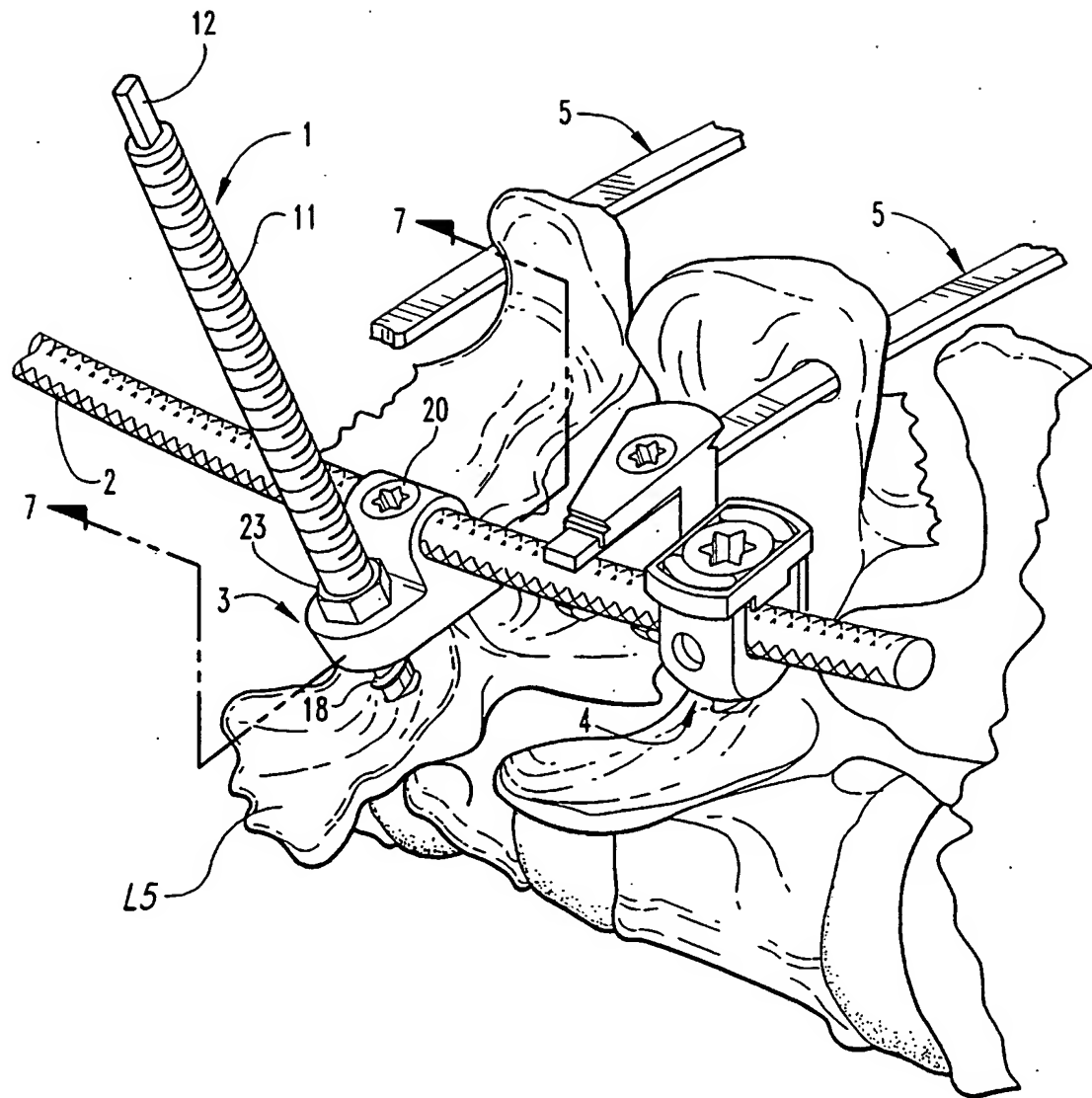
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**Fig. 5**

**Fig. 4**





**Fig. 6**



## INTERNATIONAL SEARCH REPORT

 International application No.  
 PCT/US93/10966

## A. CLASSIFICATION OF SUBJECT MATTER

IPC(5) : A61B 17/56

US CL : 606/61, 73

According to International Patent Classification (IPC) or to both national classification and IPC

## B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

U.S. : 606/60, 61, 72, 73, 104

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

## C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
X ---	US, A, 5,129,900, (Asher et al.), 14 July 1992.	1, 2, 4 -----
Y		3, 5-8
X ---	US, A, 5,147,363, (Harle), 15 September 1992, see Figure 6, element 33.	14 -----
Y		5
X ---	US, A, 3,604,487, (Gilbert), 14 September 1971.	15 -----
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Further documents are listed in the continuation of Box C.



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Date of the actual completion of the international search

07 FEBRUARY 1994

Date of mailing of the international search report

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